

Current Technology and Challenges for Medical Imaging Modalities

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Overview

- History and overview of current imaging systems
- Applications
- Challenges
- Small animal imaging challenges (Mark Henkelman)

Medical Imaging Modalities

- X-ray Imaging
- CT Scanning
- Magnetic Resonance Imaging
 - anatomical Imaging
 - functional MRI
 - fibre tract imaging
- Positron Emission Tomography
- Ultrasound

In the beginning.....X-rays

- Discovered in 1895



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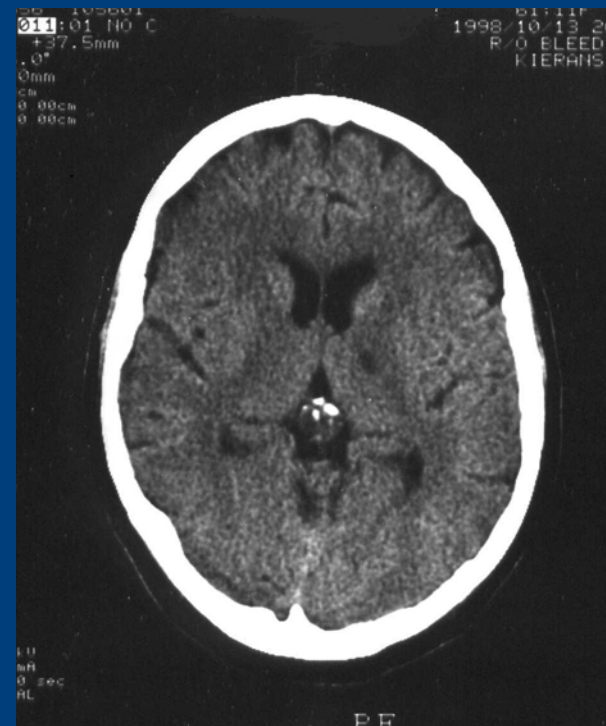
In the beginning.....X-rays

- Discovered in 1895
- Mainstay of medical imaging till 1970's



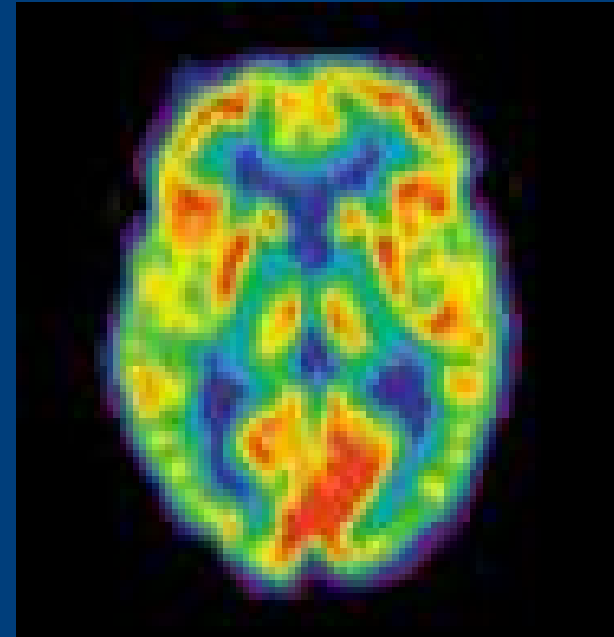
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- 1977 - PET scanning



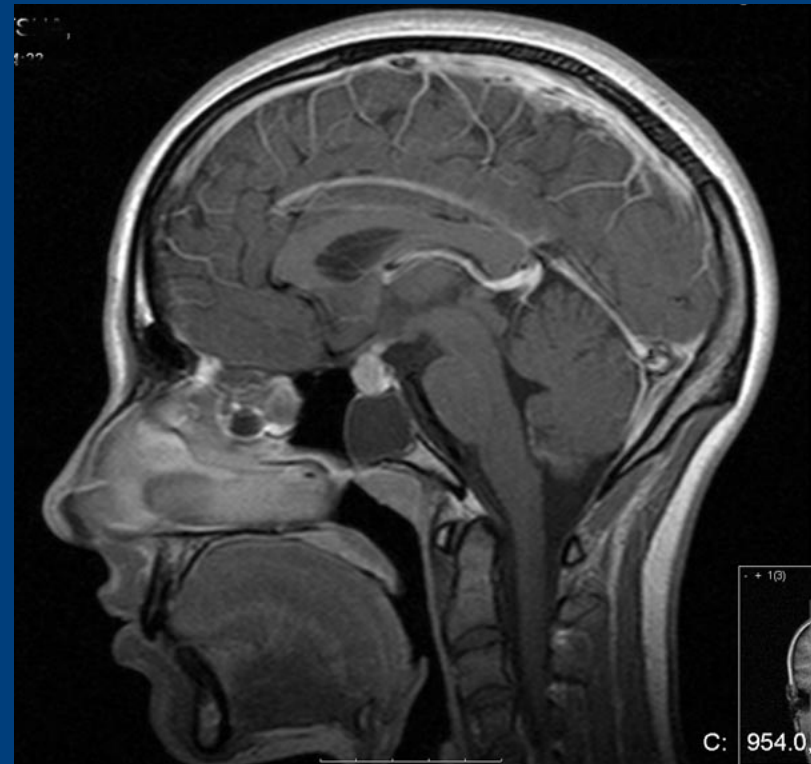
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- 1971 - CAT (CT) scanning
- 1977 - PET scanning
- 1978 - Digital Radiography



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- 1978 - Digital Radiography
- 1980 Magnetic Resonance Imaging



X-ray System



Typical X-ray system

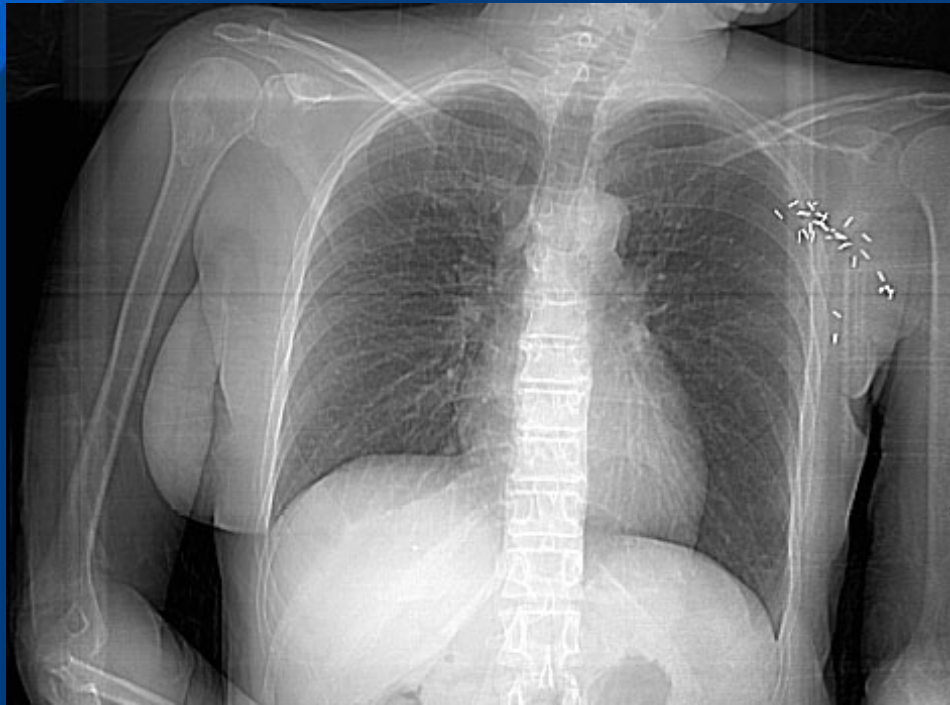
Film-screen
cassette
Screen – X-ray to
light conversion
Film – Receptor
Display
Storage



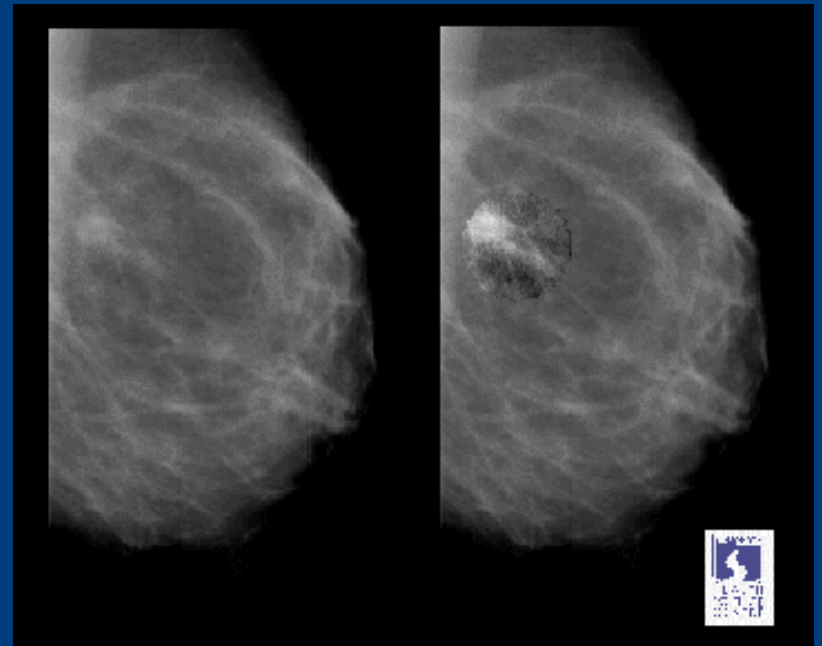
Electronic
receptor
~10MB / image



Digital radiographs

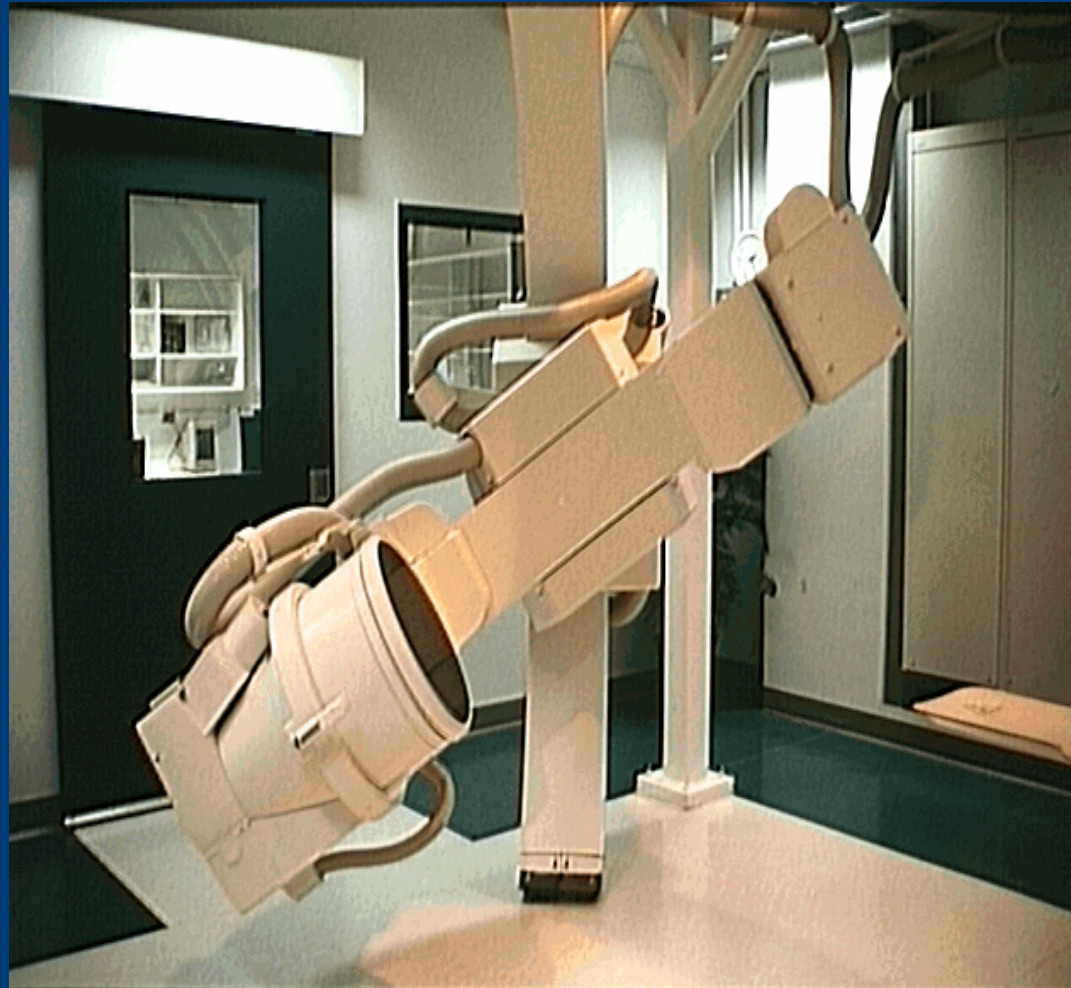


Univ Washington teaching file



Dr Martin Yaffe SWCHSC, Toronto

C-arm angiography



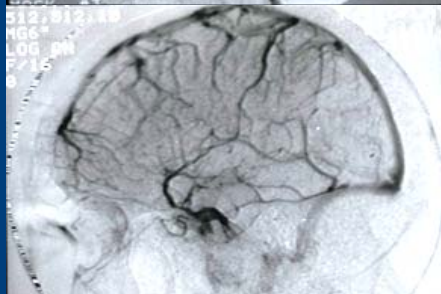
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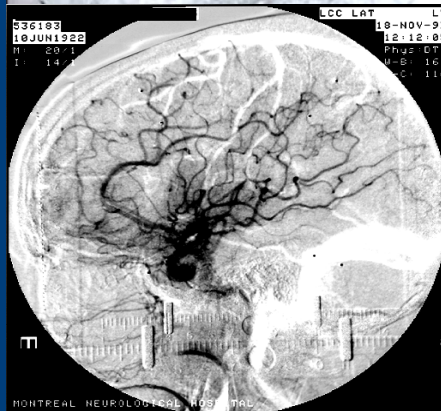
X-ray angiography - imaging vessels



Arterial



Venous



A-V

Neuro

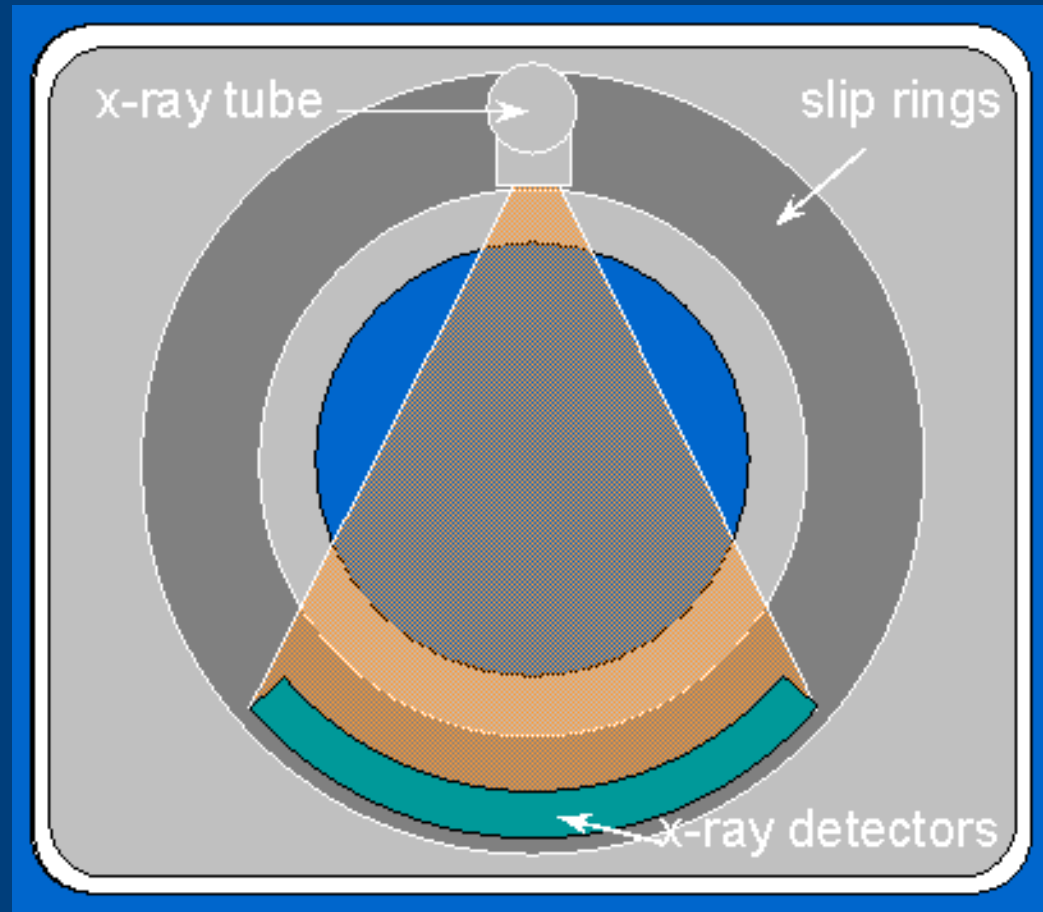


Cardiac

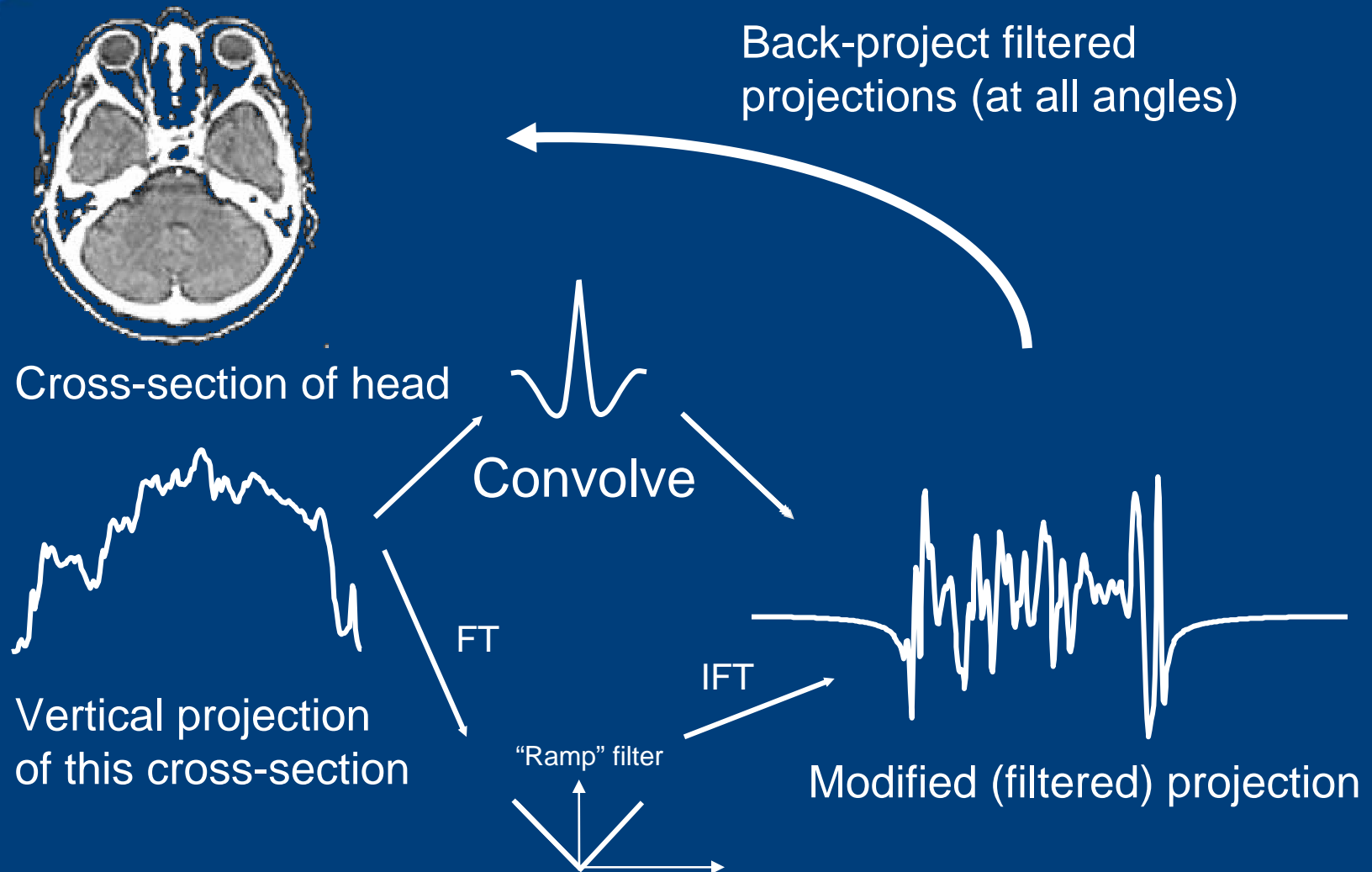
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CT Scanning

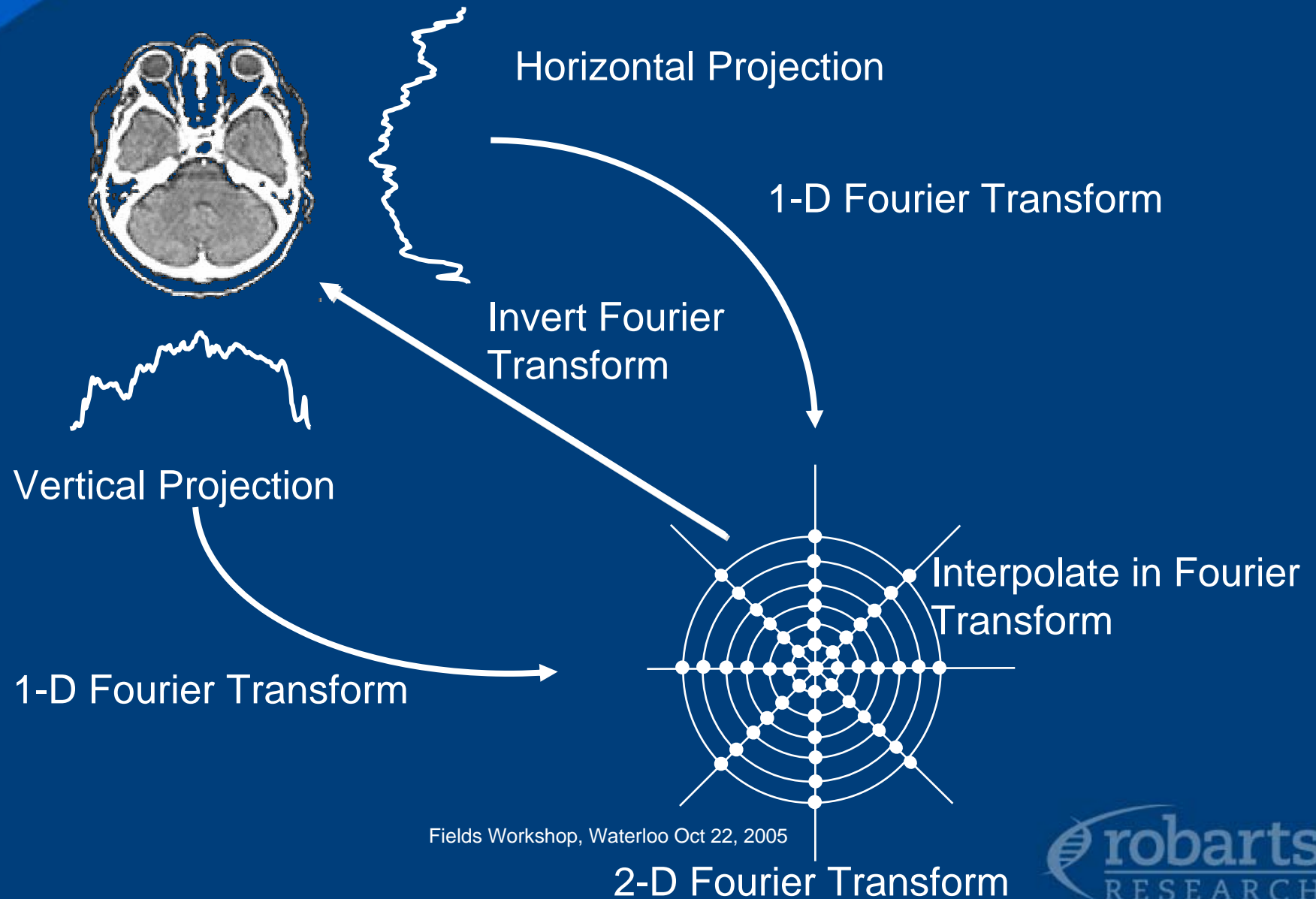
- Cross-sections using x-rays.
- Acquire projections of body from different directions
- Back-project HP filtered projections onto reconstruction plane



Back-projecting Filtered Projections

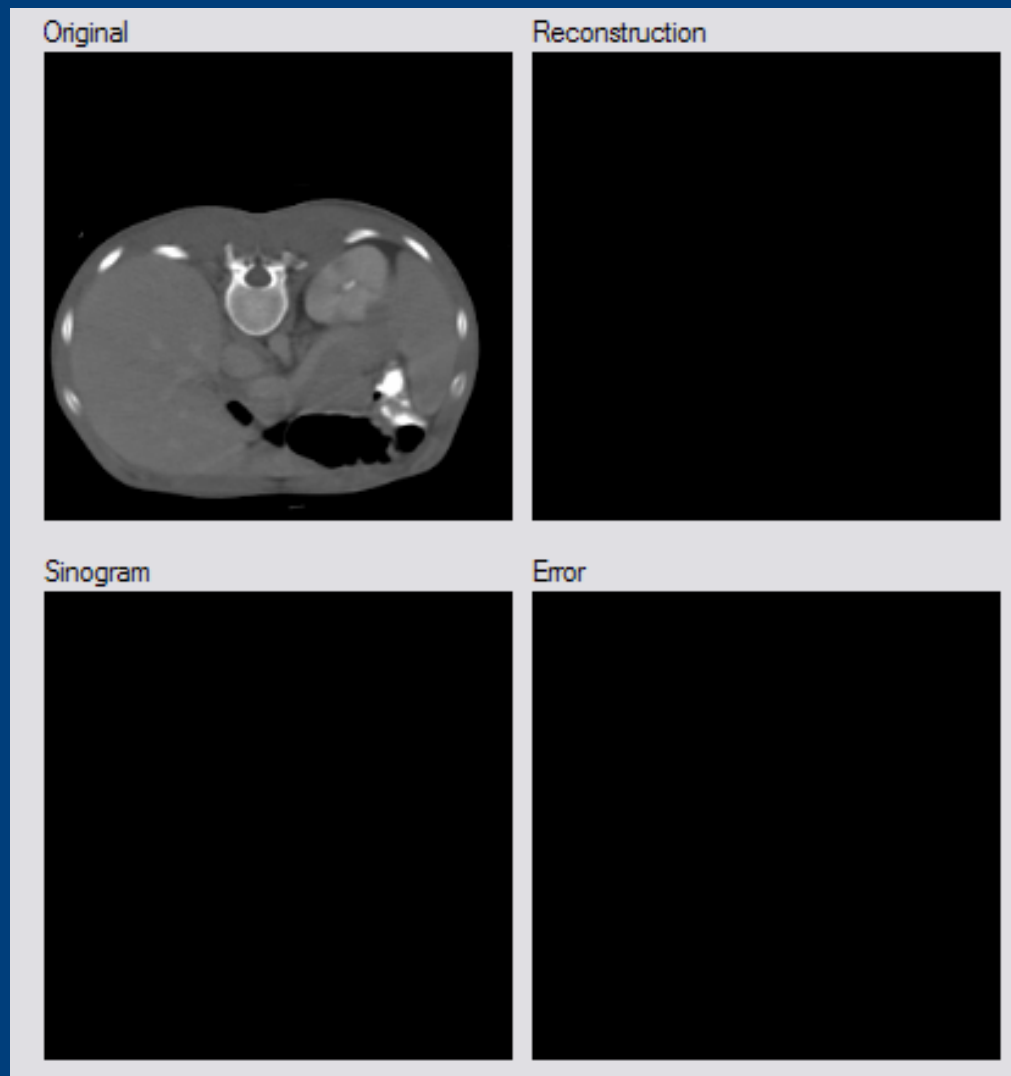


Alternative Viewpoint - Central Section Theorem



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CT Reconstruction



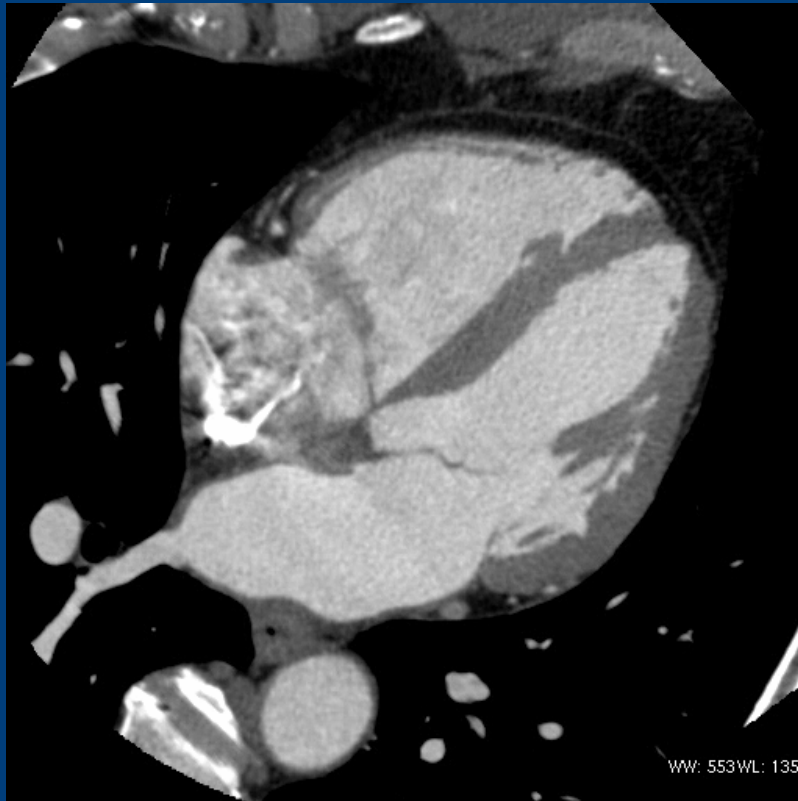
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CT Scanning

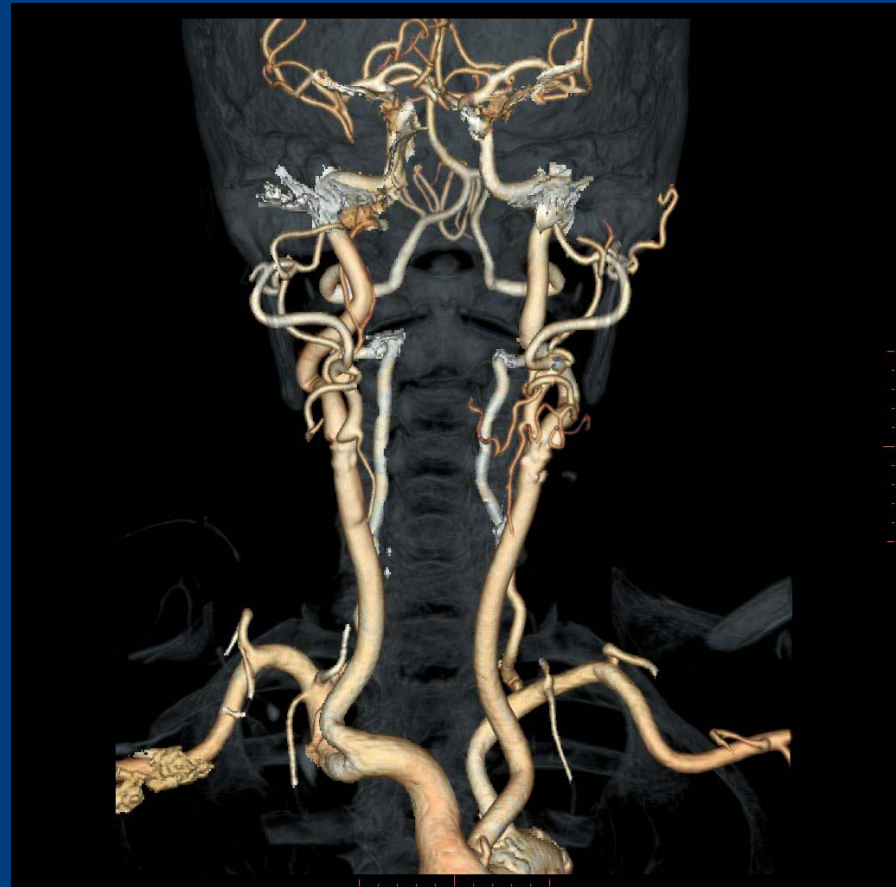
- Original
 - 80 x 80 Single or two slices
 - 4 mins acquisition time
 - 4-10 mins per slice recon
- Today
 - 64 slices simultaneously
 - < 1 sec acquisition
 - ~ .25 sec/slice recon

Dynamic CT

Beating Heart

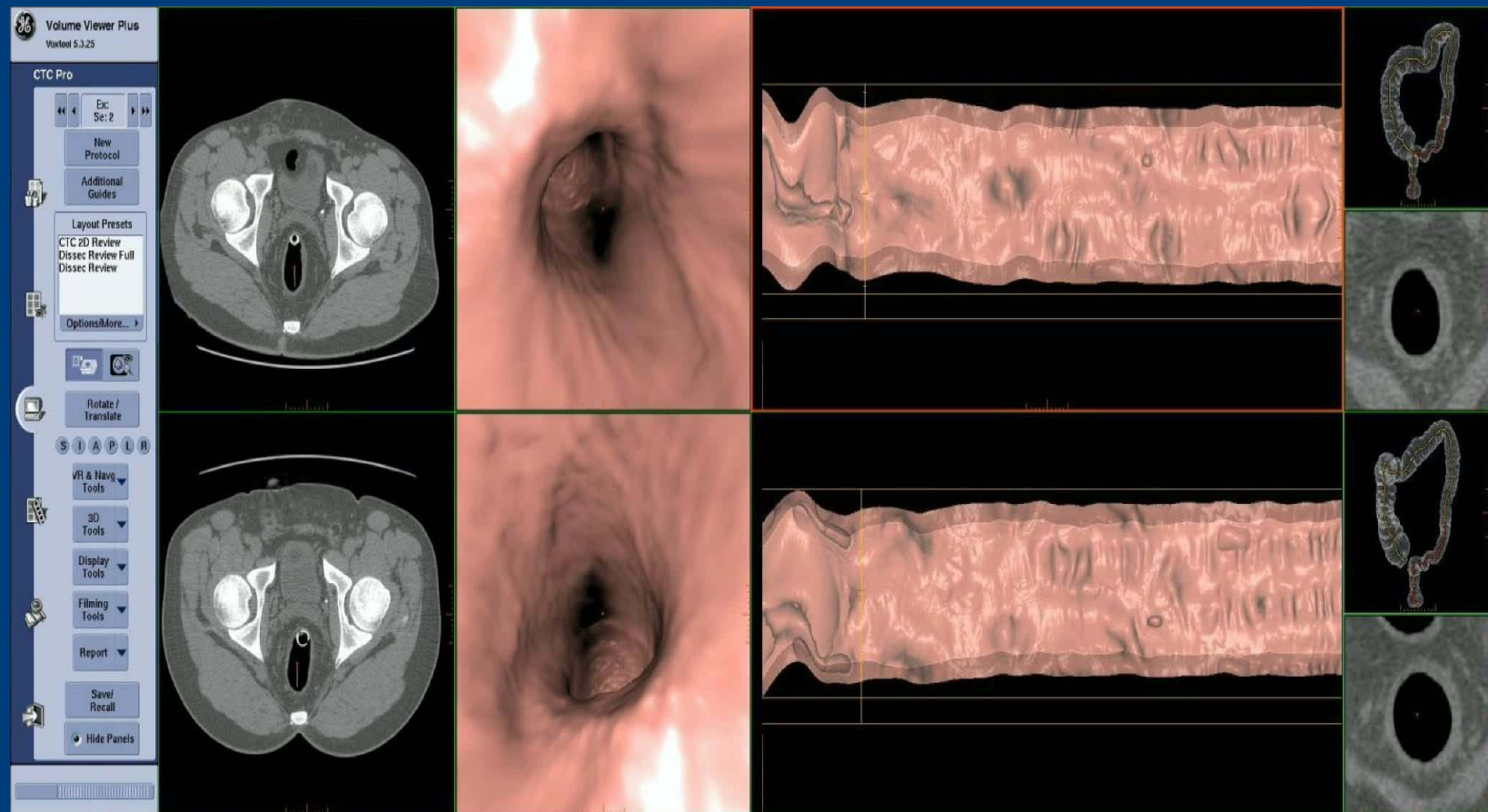


CT Angiography



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Virtual Endoscopy (colonoscopy)



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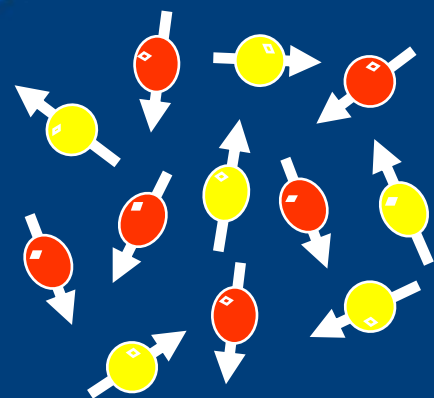
Magnetic Resonance Imaging

- Uses principles of Nuclear Magnetic Resonance (NMR)
- Roots in Physics and Chemistry labs
- Images magnetic properties of tissue
- Builds on mathematical foundation of CT
- Became MRI in medical imaging community
.... “Nuclear” considered politically incorrect!
- “Most important medical breakthrough since the invention of Xrays”

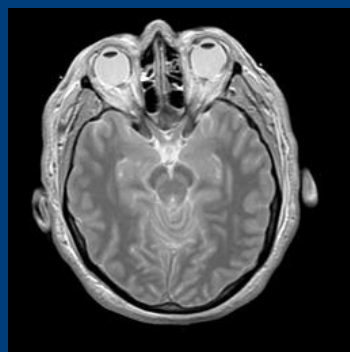
Magnetic Resonance Imaging

- H^1 nuclei wobble (precess) in a magnetic field
- Precessing nuclei emit rf signals
- Frequency of wobble depends on magnetic field
- Place body in a spatially (and time)-varying magnetic field
- Record spectrum of emitted rf signals
- Fourier transform turns these signals into an image

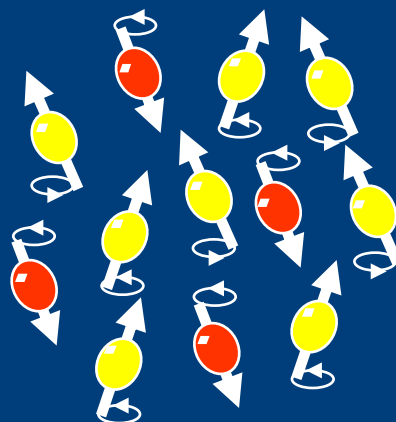
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no external field



B_0



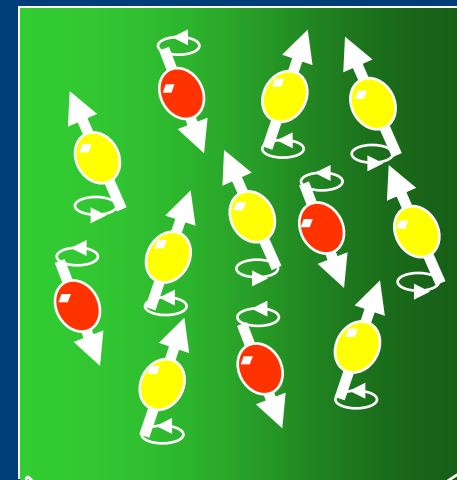
Magnetic field
and rf excitation



FT

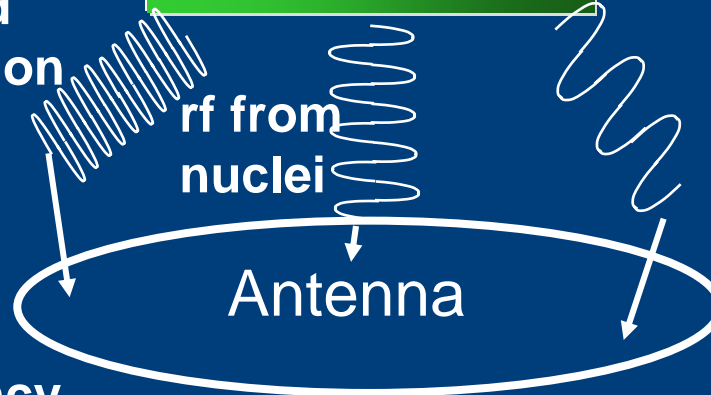
(to unscramble frequency
components)

gradient field

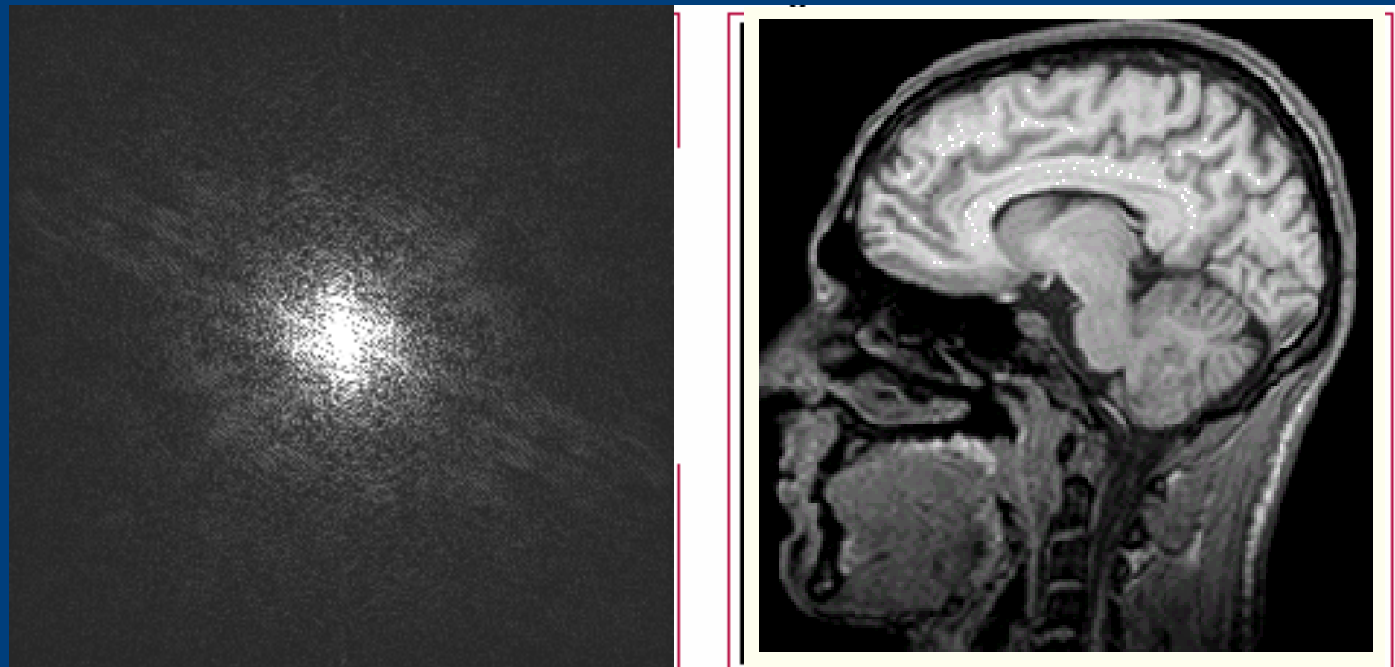


rf from
nuclei

Antenna



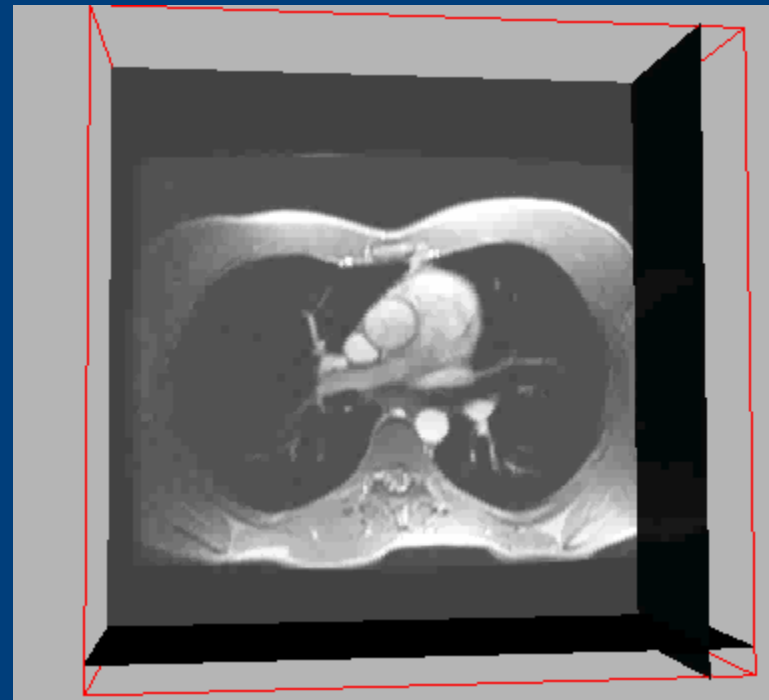
***MR data are collected in FT
domain!!!!***



FT of image (K-space)

Reconstructed image

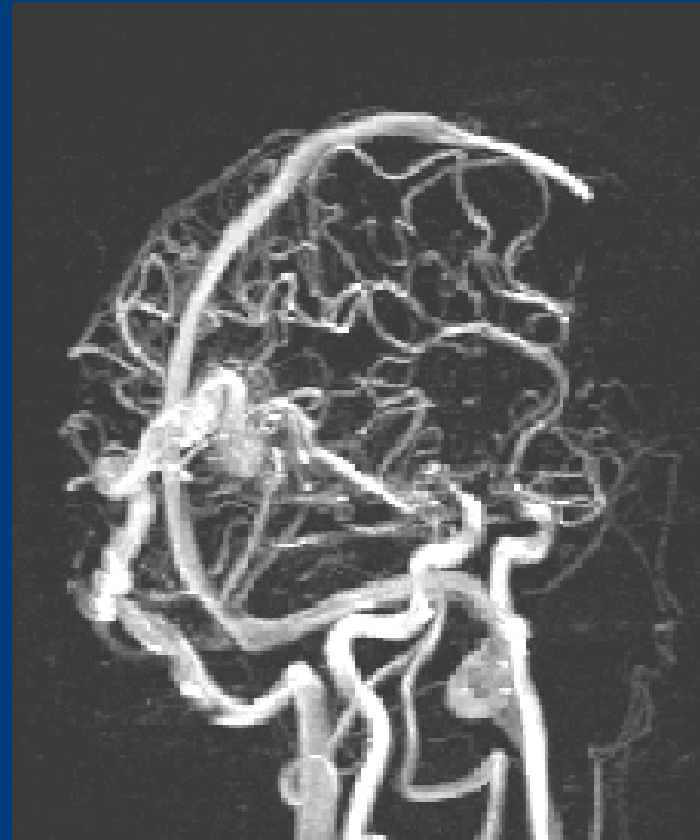
Dynamic MRI



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Magnetic Resonance Angiography

- MR scanner tuned to measure only moving structures
- “Sees” only blood - no static structure
- Generate 3-D image of vasculature system
- May be enhanced with contrast agent e.g. Gd-DTPA

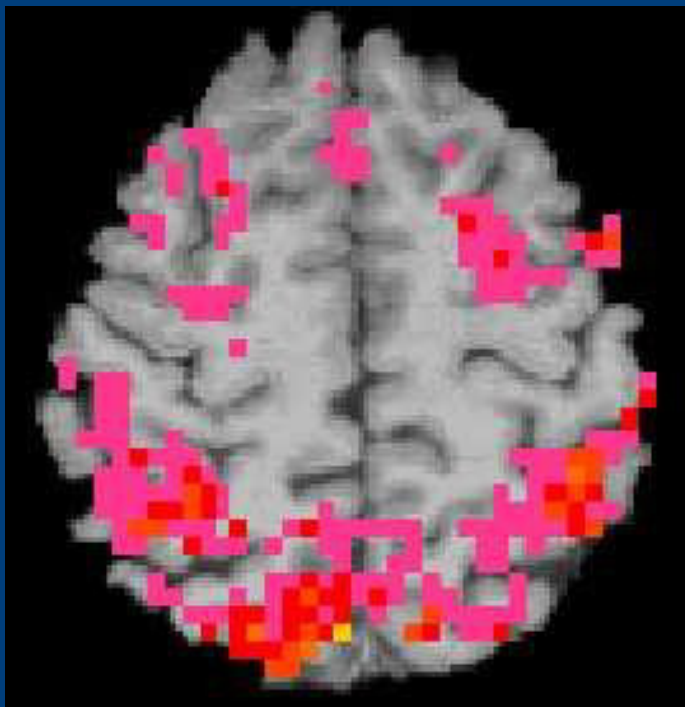


Functional MRI (fMRI)

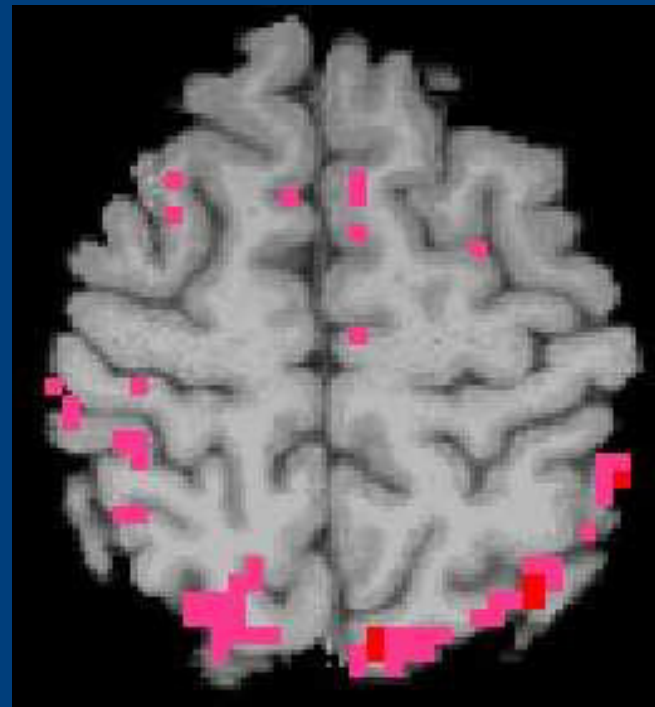
- Oxygenated and deoxygenated blood have slightly different paramagnetic properties
- Signal generated by excited protons decays more rapidly in de-oxygenated blood
- Local blood oxygenation related to brain metabolic activity
- fMRI image is map of the blood-oxygenation level dependent (BOLD) effect on anatomical MR image

fMRI

Subjects performing non-verbal working memory task:
(Mental problem solving)



Non-drinker

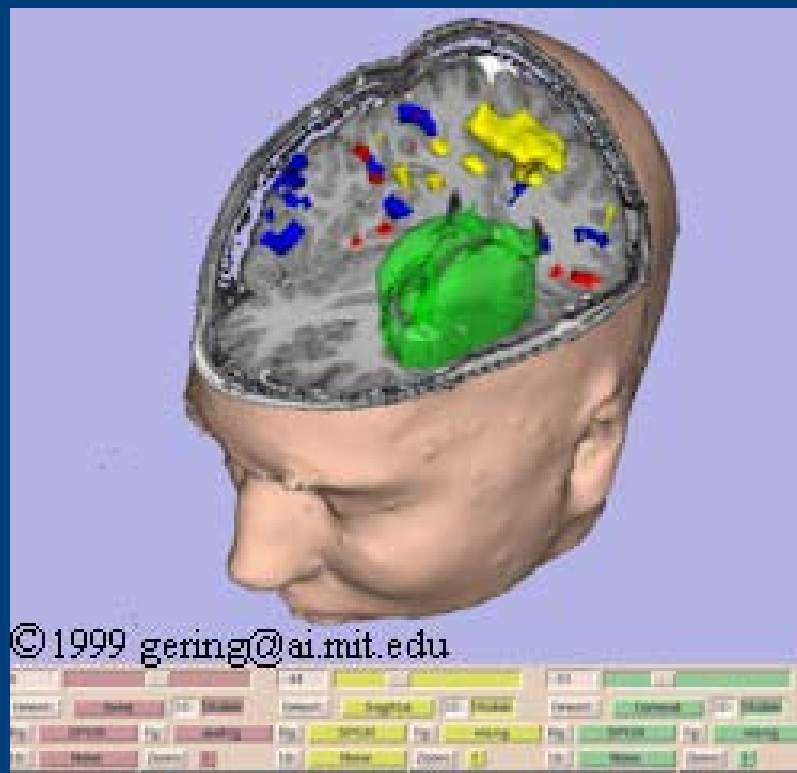


Alcoholic

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S. A. Brown, and G.G. Brown, UCSD

fMRI



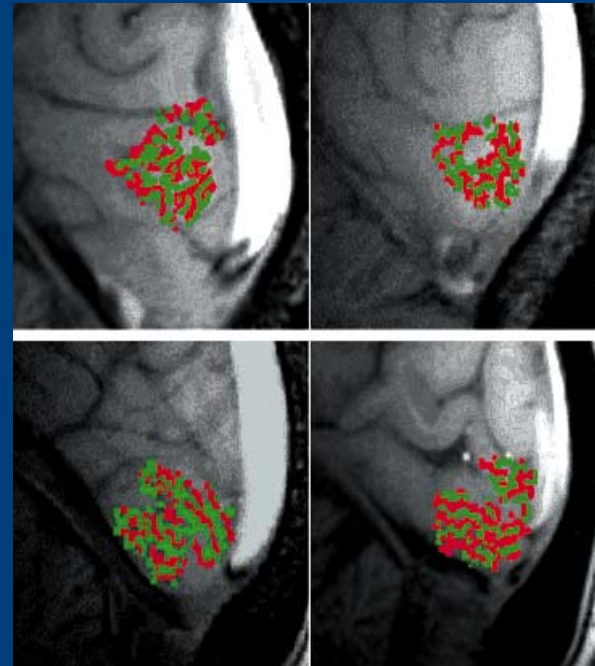
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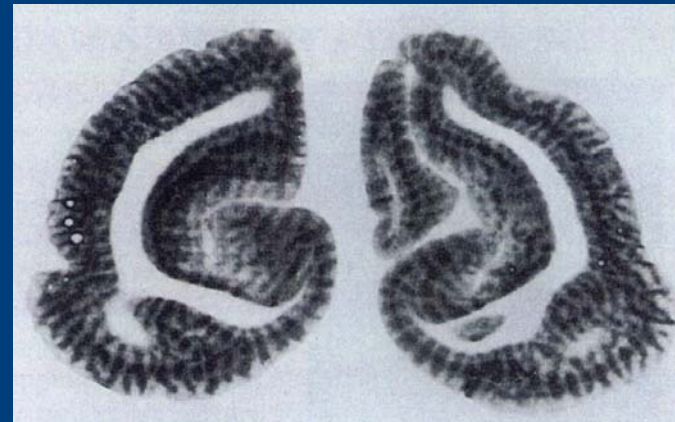
Ocular Dominance Columns



by [^3H] labeling (Hubel and Wiesel, 1977)



by Goodyear & R. Menon, 2001

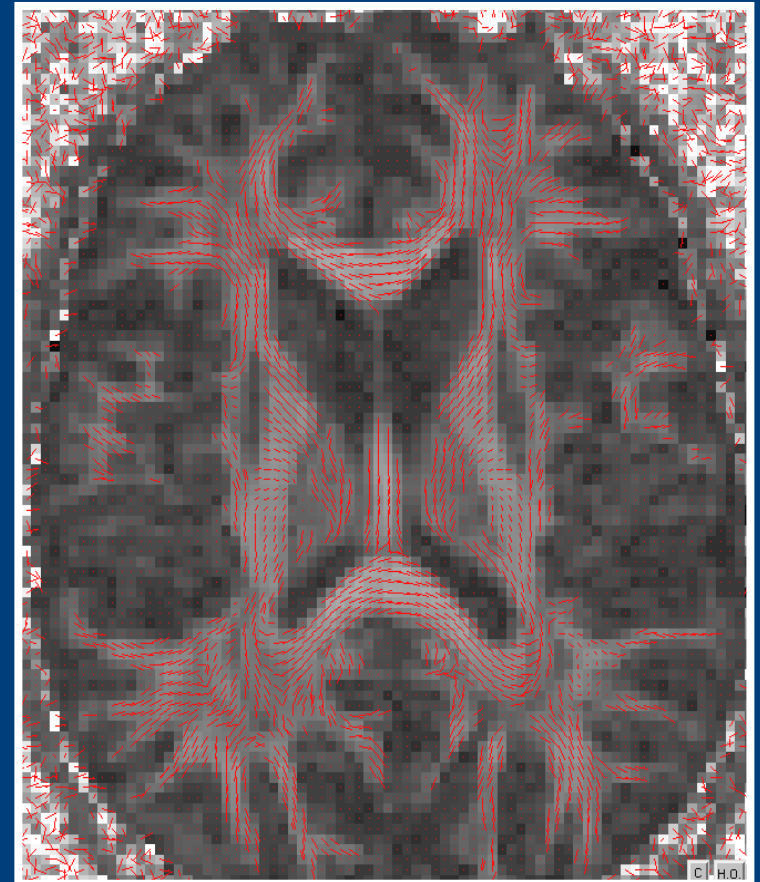


by 2- [^{14}C] deoxy-Glucose method (Kennedy et al., 1976)

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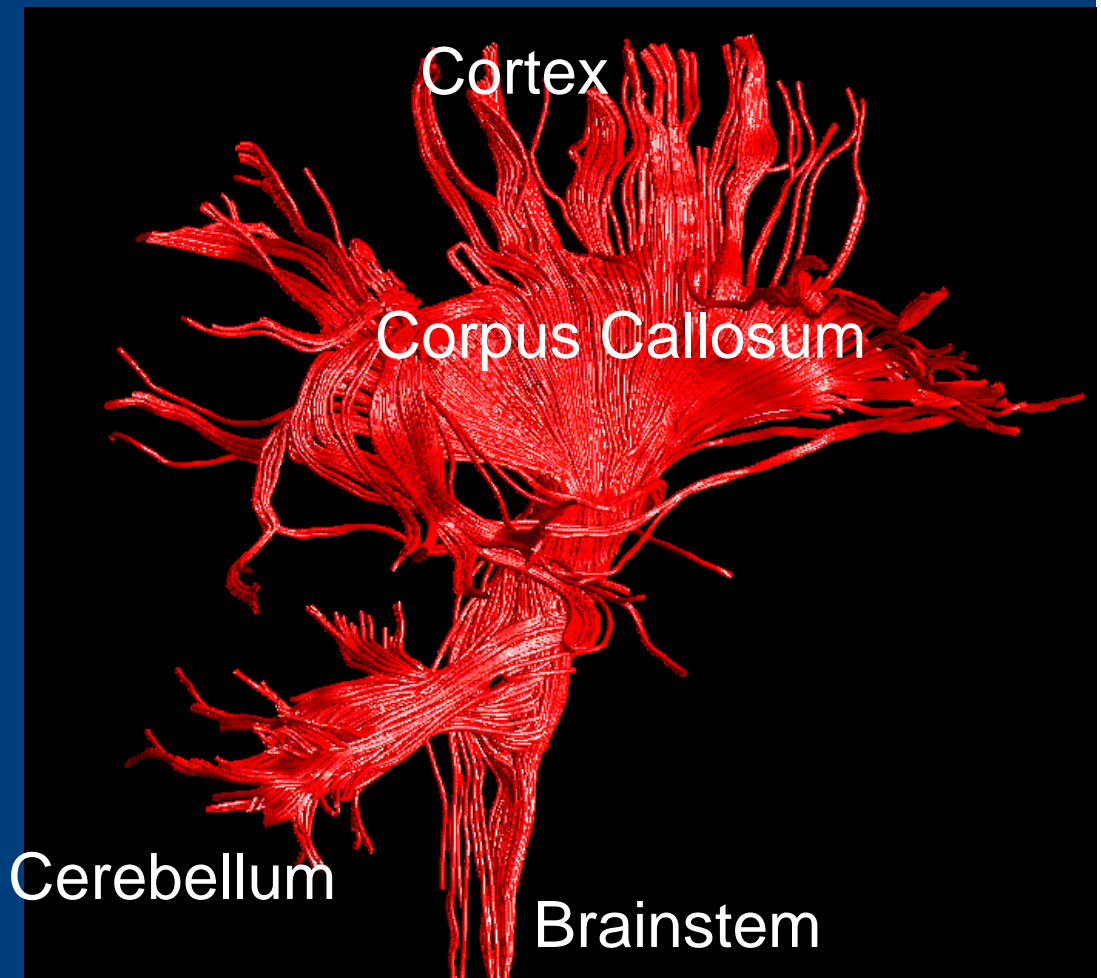
Diffusion-Weighted MRI

- Image diffuse fluid motion in brain
- Construct “Tensor image” – extent of diffusion in each direction in each voxel in image
- Diffusion along nerve sheaths defines nerve tracts.
- Connect the vectors between slices to create images of nerve connections/pathways



Tractography

- Data analysed after scanning
- Identify “streamlines” of vectors
- Connect to form fibre tracts
- 14 min scan time



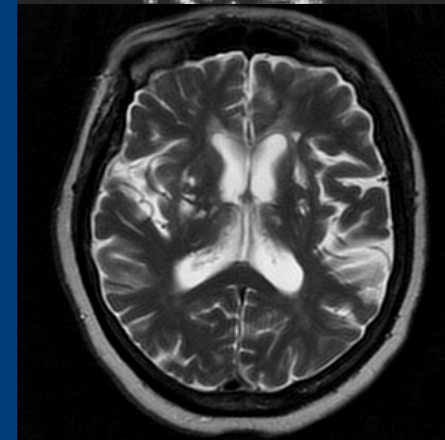
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- Dr. D Jones, NIH

30 Years of MRI



First brain
MR image



Typical T2-
weighted MR
image today

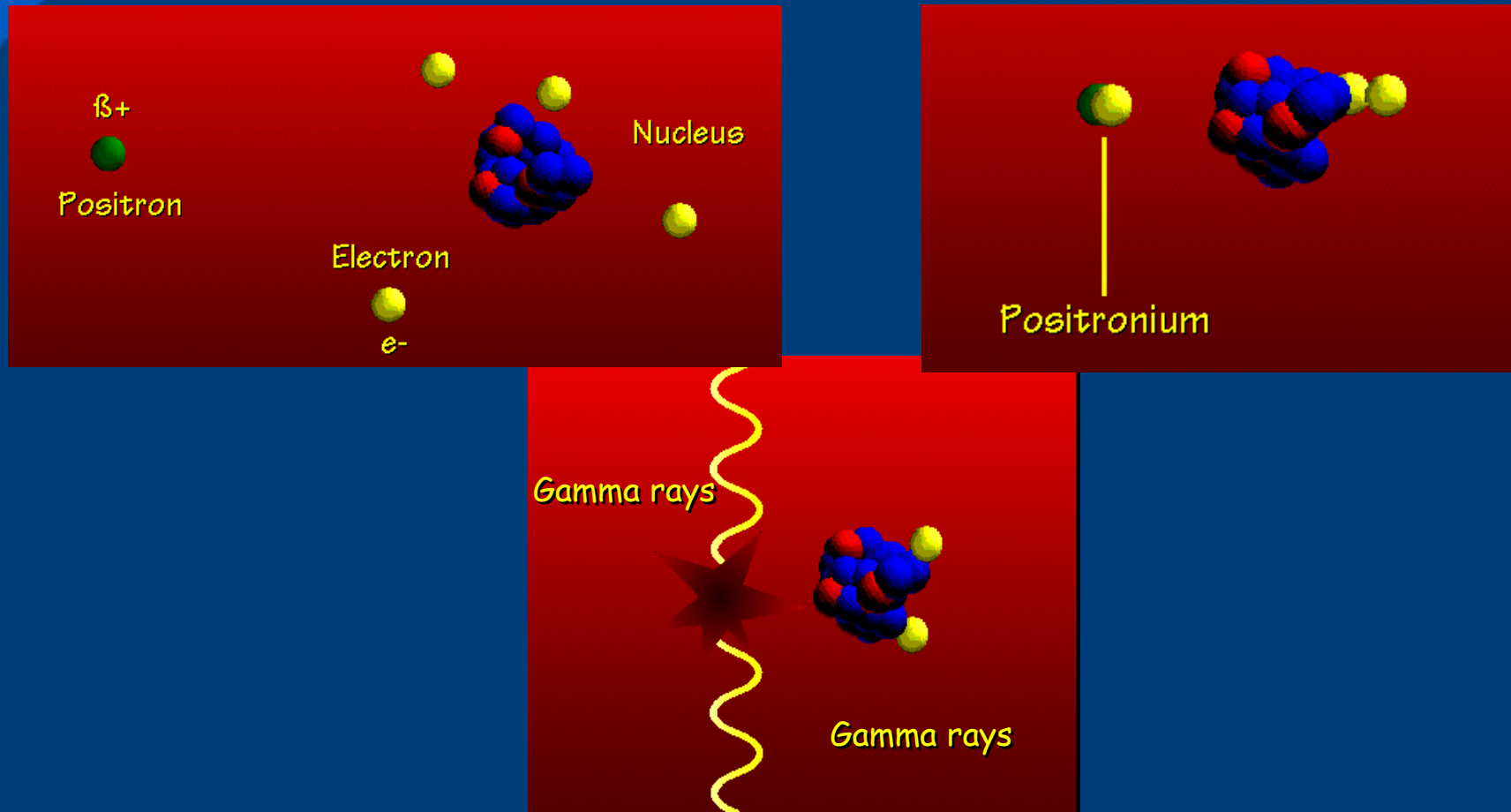
MRI

- 20 years ago
 - Single slice
 - .5 – 2 mins per slice
- Today
 - Sub-second per slice
 - Volumetric imaging
 - (Still 30 mins for volume image of beating heart – involves breath-hold)

Positron Emission Tomography

- Inject metabolically active positron emitting isotope
- Positron interacts with electron
 - Mutual annihilation
 - 511 keV gamma rays emitted
- Coincidence detection in opposing detectors give line on which annihilation occurred
- Multiple lines used in CT- style reconstruction

Positron Annihilation

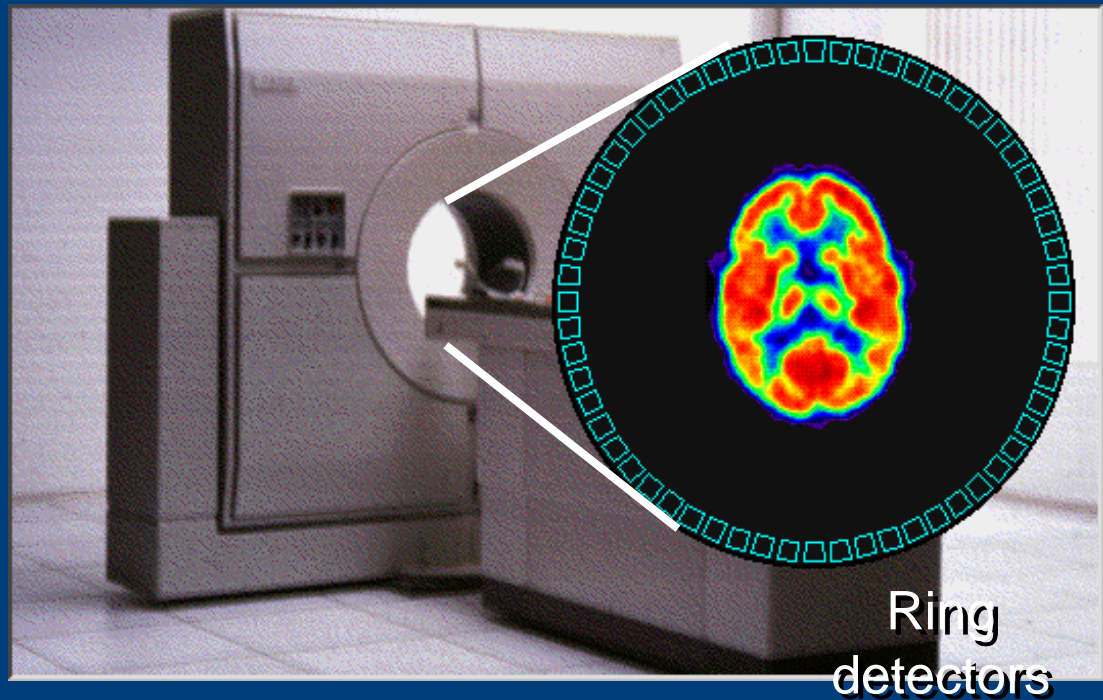


Crump Institute for Biological Imaging UCLA

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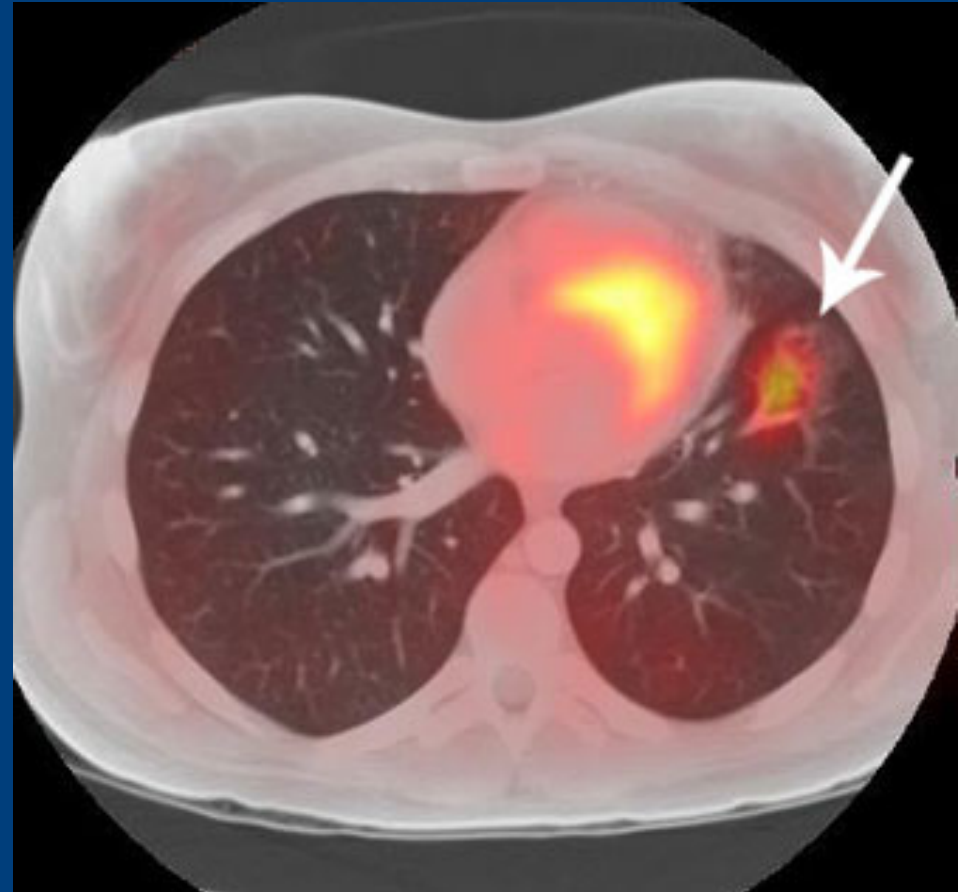
PET Scanning

- Track dynamics of radio-labeled metabolites
- Quantitative analysis of metabolic function
- Detect abnormal organ function



PET-CT

- Pet scanner and CT combined in same unit
- PET provides function
- CT provides anatomy
- Intrinsic registration between both images
- CT image aids reconstruction of isotope distribution



3-D Animal CT

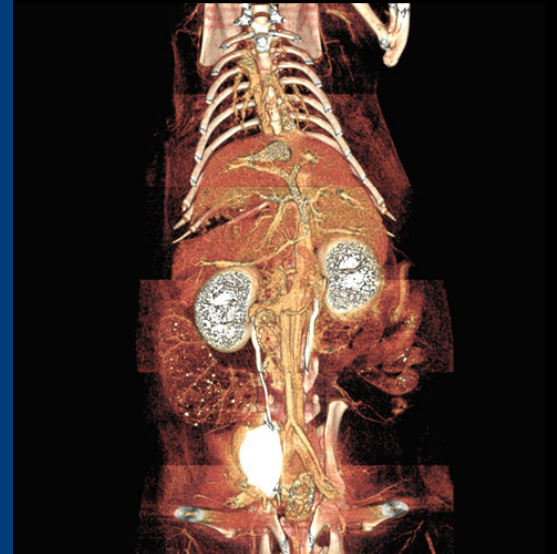
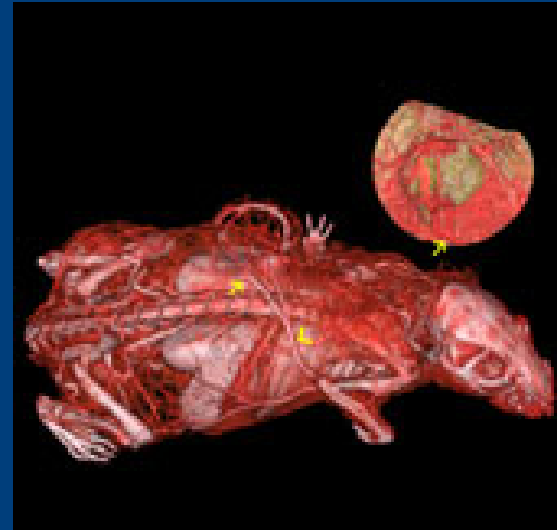


Bench-top scanner for
animal specimens



Scanner for live animals

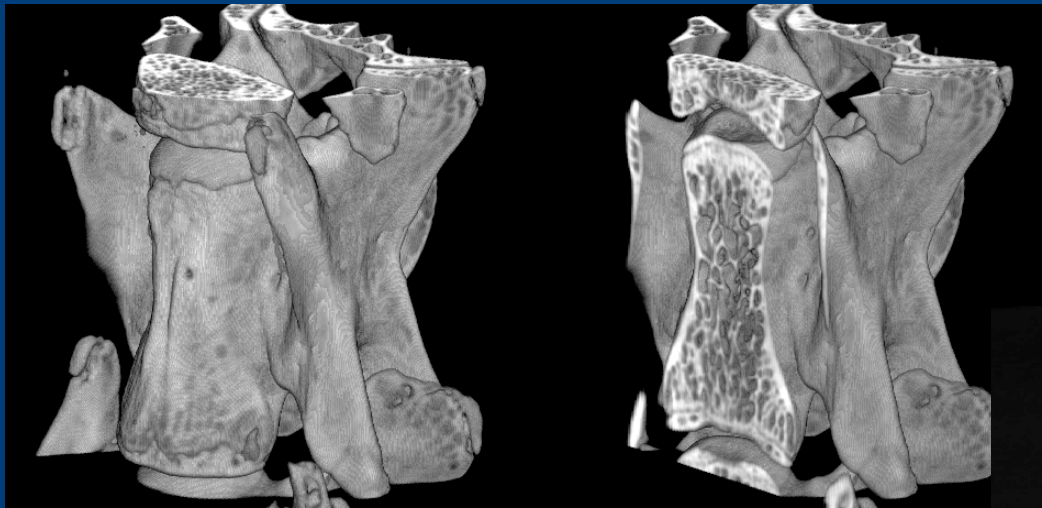
CT mouse Scans



GE Health Systems

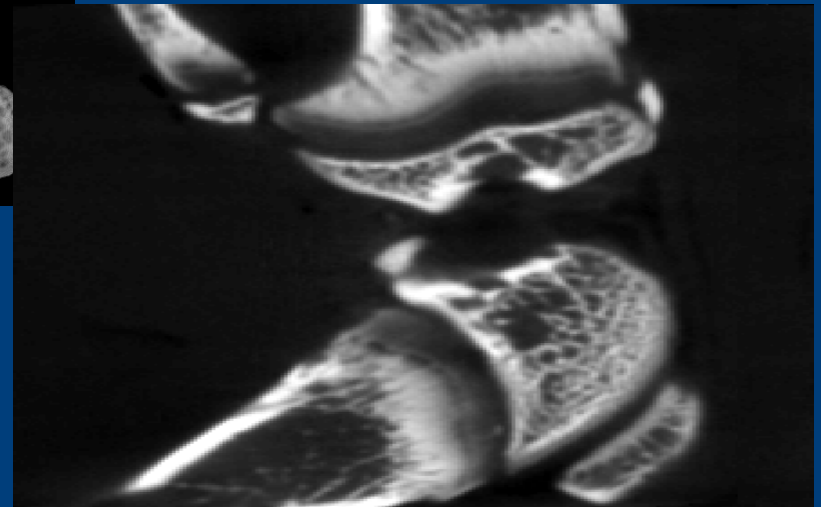
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Results: in vitro 3-D μ CT

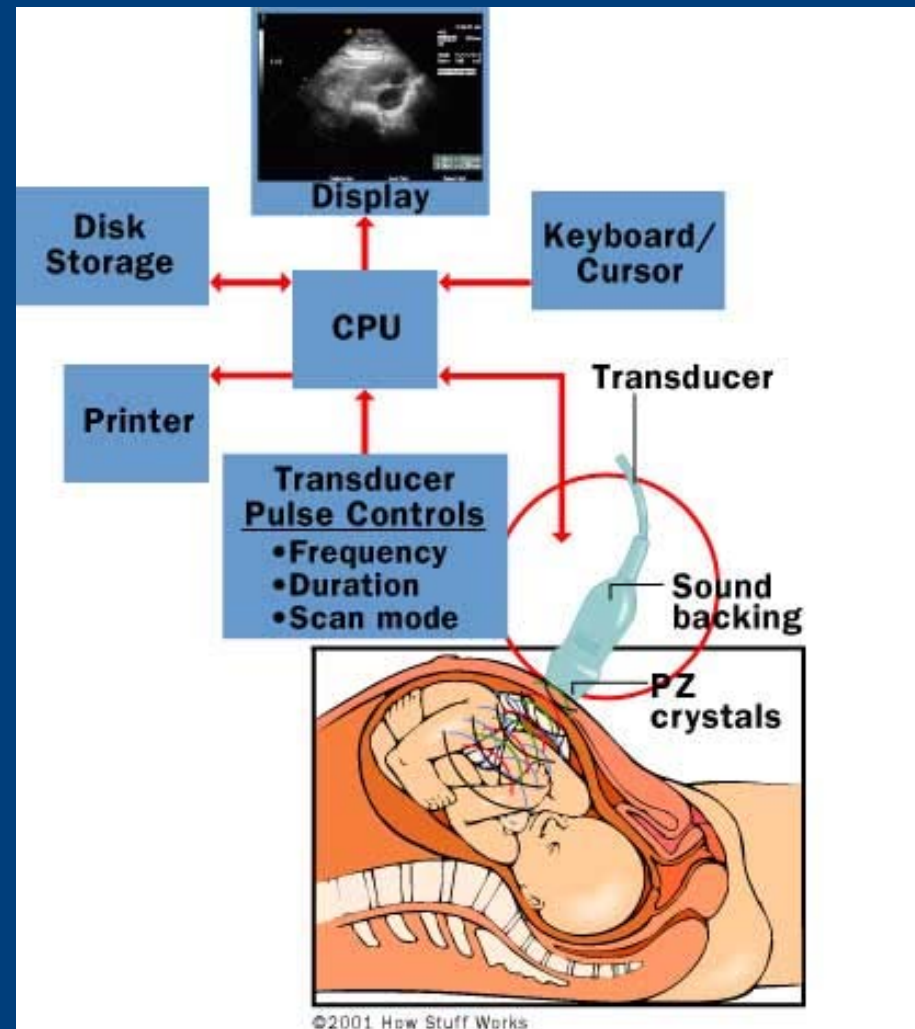


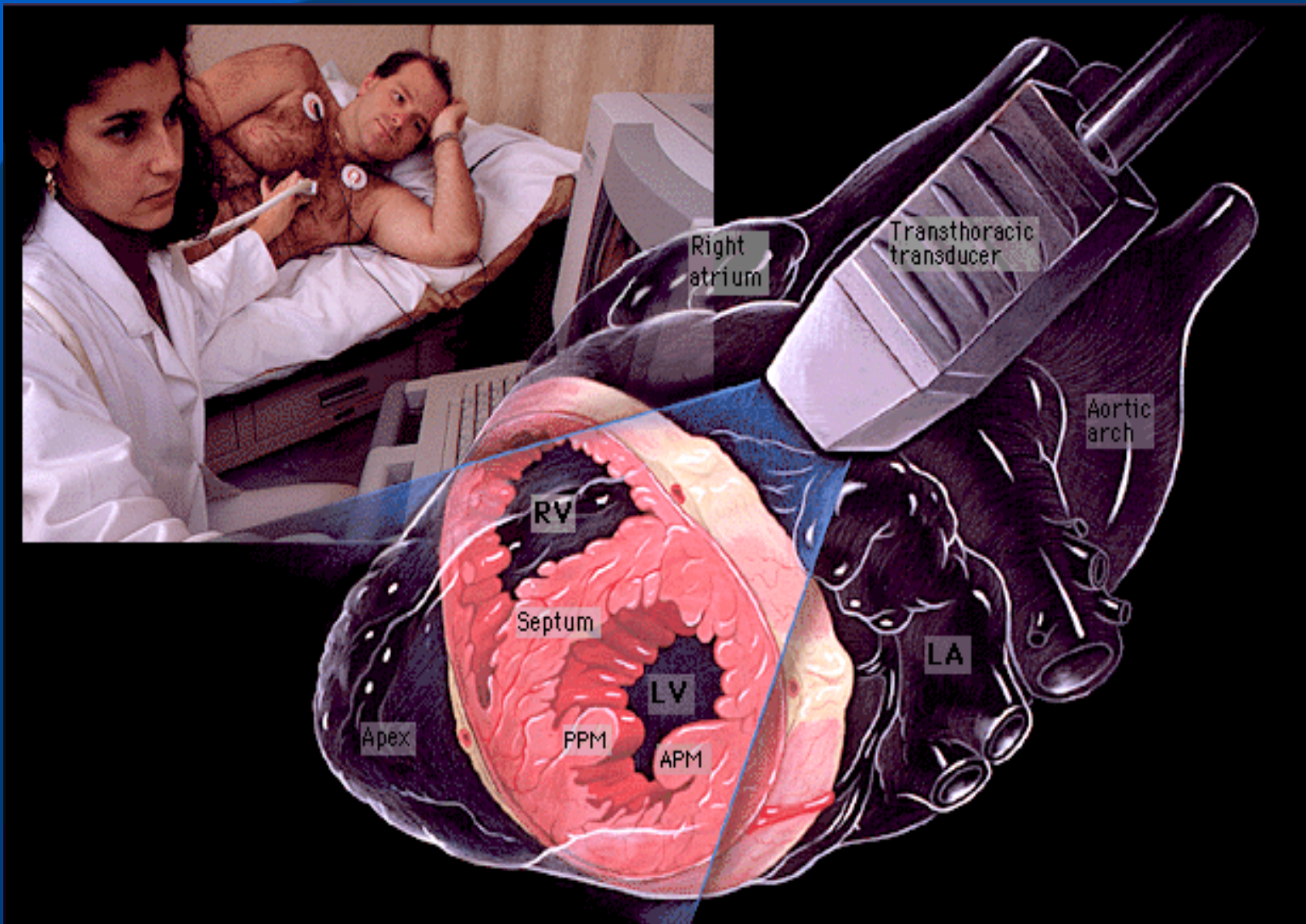
~20 μ m resolution

David Holdsworth RRI



Ultrasound





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Acquisition time: 20 min

1989: 2D ultrasound used most often, taking about 20 minutes for U/S to develop and image, until 3D was invented



4 vol / sec

1995: Live 3D introduced, speeding up the time it took for an image to appear and beginning to show movement

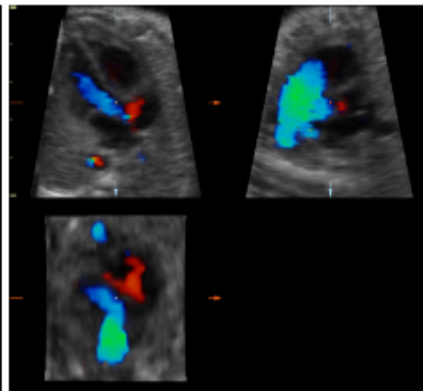
2000



16 vol / sec

2000: Improvements in ultrasound technology led to a faster time to acquire an image, creating a more "life-like" appearance of fetal anatomy

2005



33 vol / sec

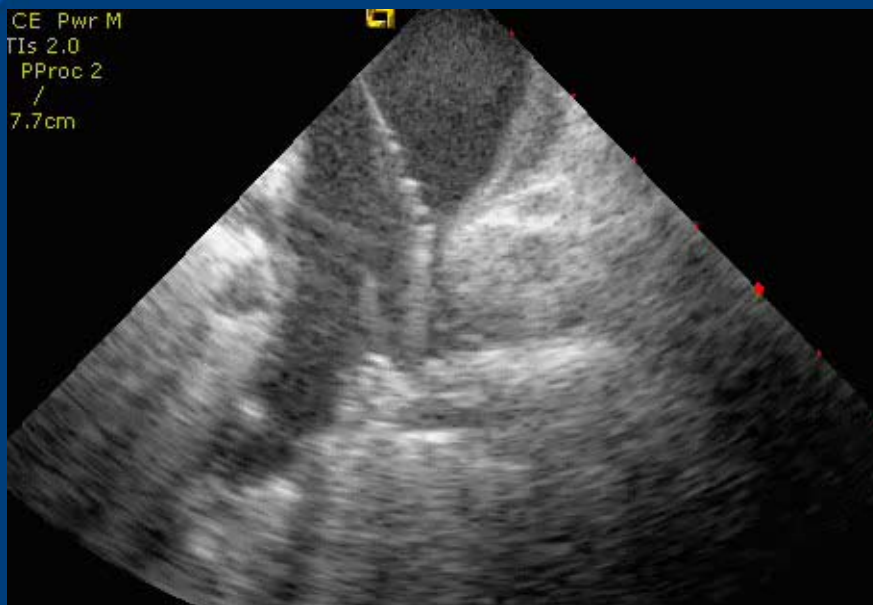
2005: Advancements in 3D and 4D ultrasound expands the usefulness of ultrasound into areas like viewing the fetal heart and blood flow

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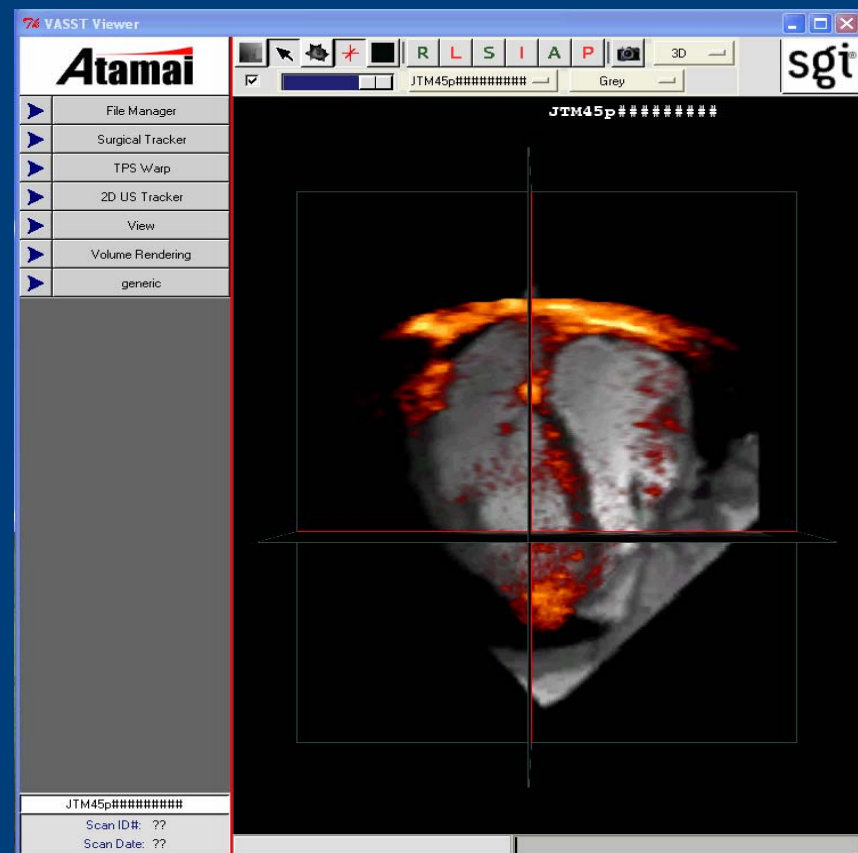


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Cardiac ultrasound



Intra-cardiac echo



Registered with MRI

MRI

- Generally non-invasive (but new contrast agents are not!)
- Solid tissues like bone are “transparent” as signal is due to H_2O content in tissue
- Generally well tolerated with excellent safety
- Functional aspects of tissues can be determined like blood oxygenation in brain in response to stimuli
- Excellent diagnostic characteristics of tumour and other tissues due to differences in H_2O environments
- Geometrical accuracy can present problems for surgical guidance
- Need: Volumetric dynamic scanning

CT

- Very high resolution
- Intrinsic geometrical accuracy
- Isotropic imaging with modern multi-detector spiral scanners $(0.5\text{mm})^3$ voxels
- Full volume scan in several seconds
- Excellent bone contrast
- Poor soft-tissue contrast
- Vascular images with contrast agent
- “Real-time” (5-10 fps) single slice “fluoro mode”
- Need: faster scanning at lower dose

Ultrasound

- Inexpensive, portable
- Real-time
- 2D and 3D dynamic
- Images sonic interfaces between tissues
- Cannot penetrate bone/air
- Geometrical accuracy limited by US refractive index changes
- Often only choice for intra-operative imaging
- Need: miniature 4D transducers

Data Storage and Analysis

- Dynamic Cardiac CT
 - $512^3 \times 20$ (5.2 GB)
- Dynamic MRI
 - $256^3 \times 15$ (0.5 GB)
- Micro CT of Mouse
 - ~0.4 GB

Visualization

- Data must be visualized efficiently
- Interacting with GB datasets in a dynamic image is major challenge
- Effectively combine multimodal data
- Employ combination of surface, volume and texture mapping
- Use capabilities of HW graphics boards.

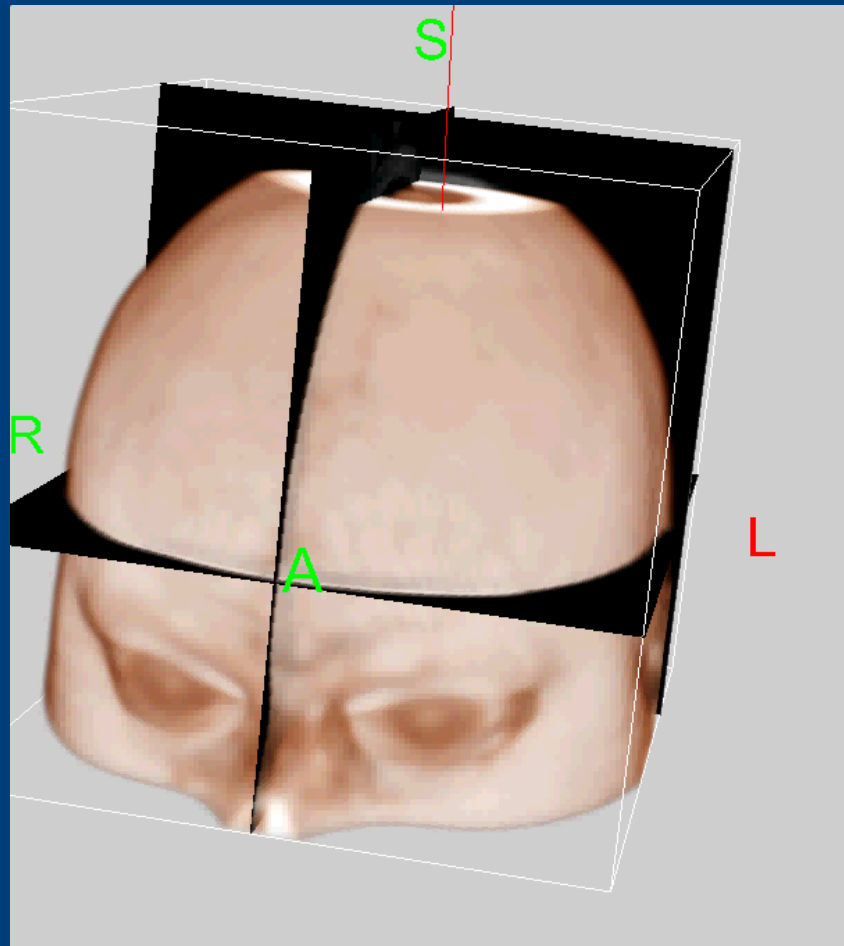
Navigating the functional brain!

“Wow! That was a good one! Try it – just poke his brain where my finger is!”



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Applications in Image-Guidance



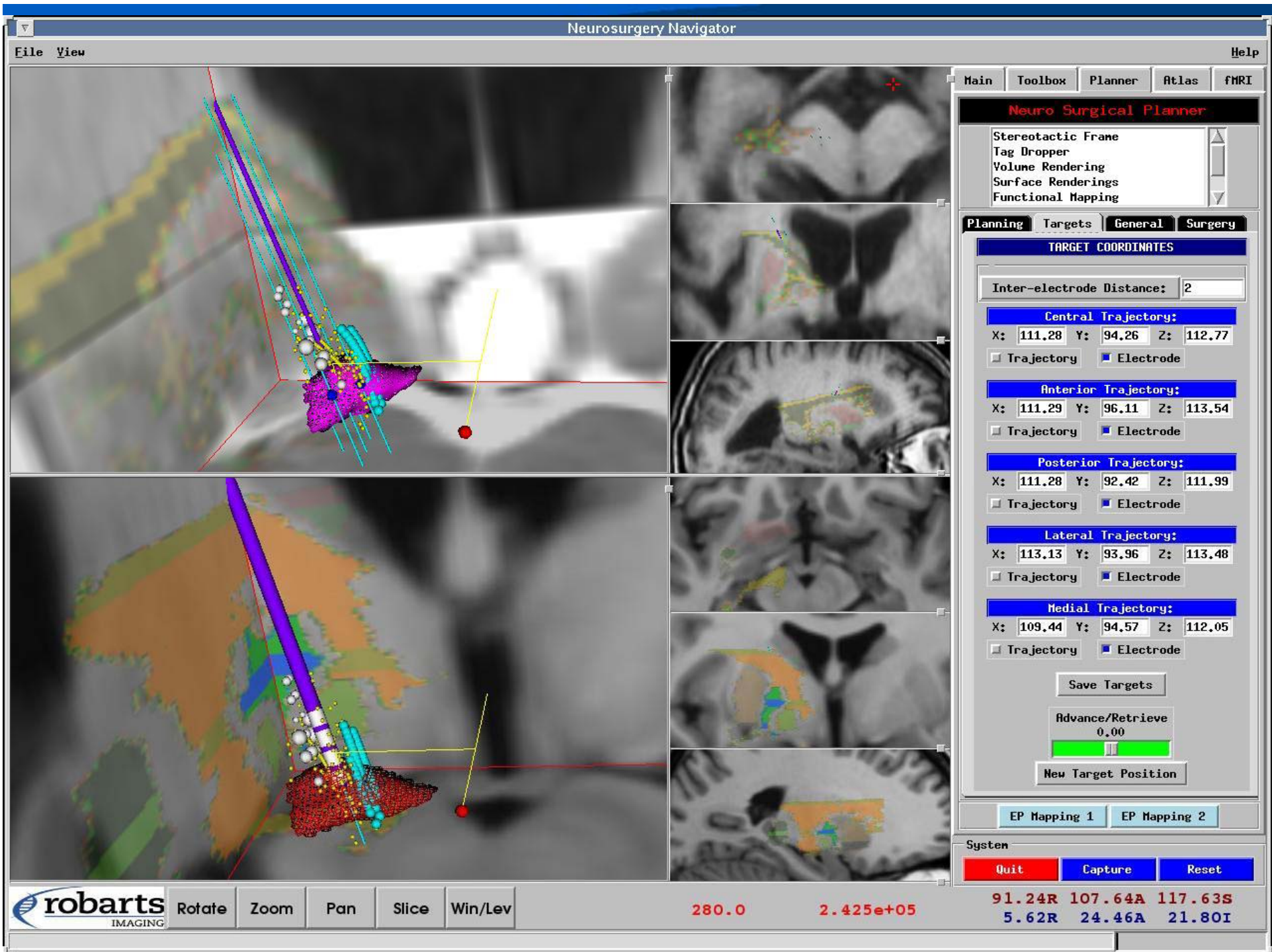
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Non-rigid brain registration

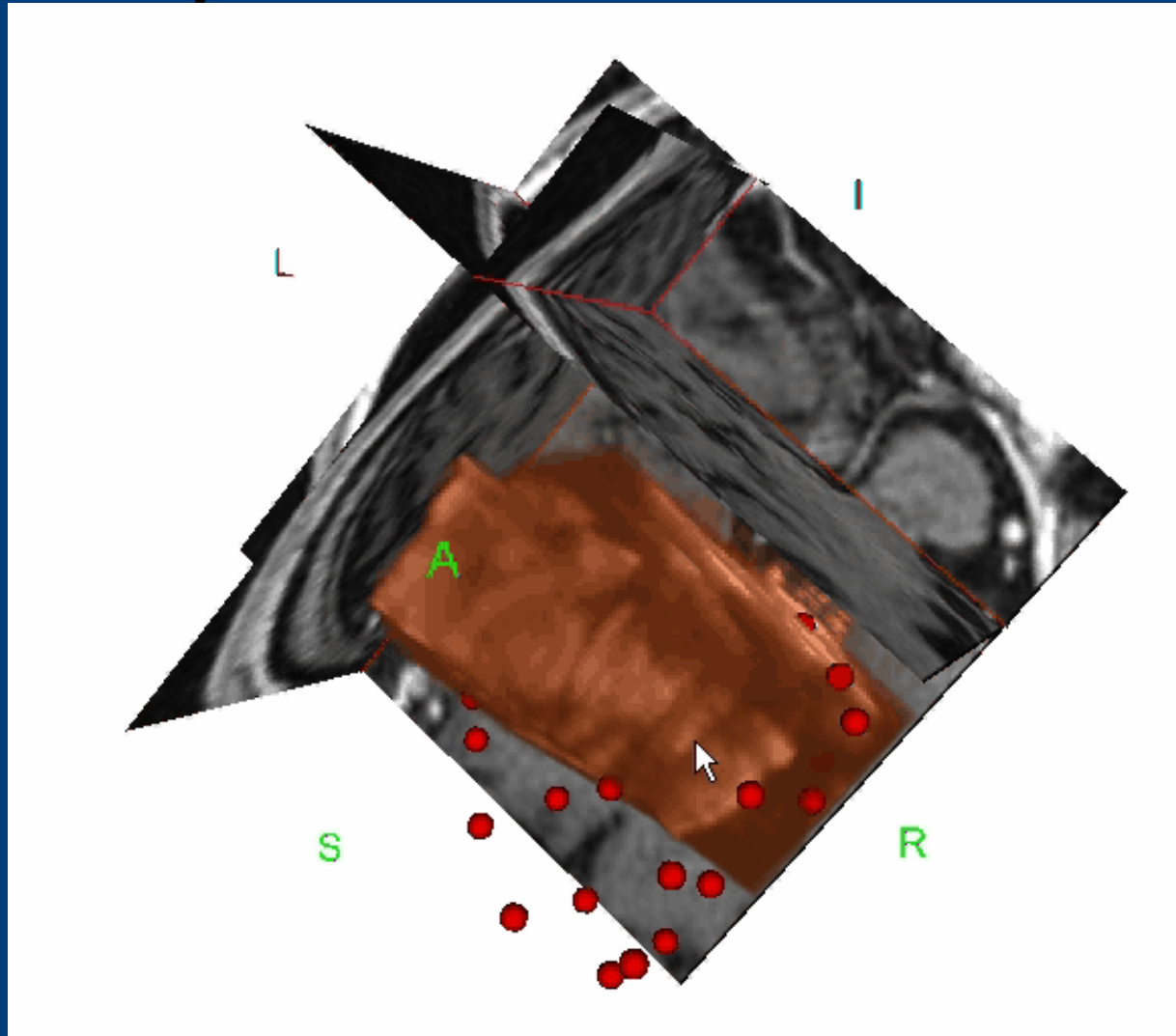
- Map atlases from standard brain to patient
- Collect EP data from multiple patients in standard image volume
- Map EP database to patient



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Intra-Operative MR/US warp



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Challenges

- Ready availability of 3D/4D datasets in viewing room/OR
- Cross reference to other images of same patient
- Rapidly interrogate hi-res 3D dynamic images
- Integrate with surgical guidance

Computational Challenges

- The fusion of image data of varying modalities, over differing spatial and temporal scales and resolutions
- The extraction and display of quantitative information, with associated uncertainties
- Data archiving: raw vs. extracted parameters, development of metadata standards

*Report commissioned by DOE and NIBIB

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An example - Image-guidance for Cardiac surgery

- Register pre-operative, intra-op images to patient
- Synchronize pre- and intra-op images
- Track instruments and register to dynamic environment
- Visualize and interact with volume

